Comparison of 3D and 2D characterization of spinal geometry from biplanar X-rays: a large cohort study

Zongshan Hu¹², Claudio Vergari³⁴, Laurent Gajny⁴, Zhen Liu¹, Tsz-Ping Lam²³, Zezhang Zhu¹⁺³, Yong Qiu¹⁺³, Gene C. W. Man²³, Kwong-Hang Yeung³⁵, Winnie C. W. Chu³⁵, Jack C. Y. Cheng²³, Wafa Skalli⁴

¹Department of Spine Surgery, Drum Tower Hospital of Nanjing University Medical School, Nanjing, China; ²Department of Orthopaedics and Traumatology, The Prince of Wales Hospital, The Chinese University of Hong Kong, Hong Kong, China; ³The Joint Scoliosis Research Center of the Chinese University of Hong Kong-Nanjing University, Faculty of Medicine, The Chinese University of Hong Kong, Hong Kong, China; ⁴Arts et Métiers Institute of Technology, Université Sorbonne Paris Nord, Institut de Biomécanique Humaine Georges Charpak (IBHGC), HESAM Université, Paris, France; ⁵Department of Imaging and Interventional Radiology, The Prince of Wales Hospital, The Chinese University of Hong Kong, Hong Kong, China

These authors contributed equally to this work.

Background: Biplanar X-ray system providing anteroposterior and sagittal plane with an ultra-low radiation dose and in weight-bearing position is increasingly used for spine imaging. The original three-dimensional (3D) reconstruction method from biplanar X-rays has been widely used for clinical parameters, however, the main issue is that manual adjustments of the 3D model was quite time-consuming and limited to thoracolumbar spine. A quasi-automated 3D reconstruction method of the spine from cervical vertebra to pelvis was proposed, which proved fast and accurate in 57 patients with adolescent idiopathic scoliosis. The aim of this study was to compare the newly developed technique of quasi-automatic 3D measurement with classical 2D measurements in a large cohort.

Methods: A total of 494 adults with biplanar EOS X-ray scanning were included in this study and divided into health and deformity group according to the presence of spinal deformity. The proposed method of quasi-automatic 3D measurement was applied to all these subjects. The radiographic parameters included: thoracic kyphosis (TK), lumbar lordosis (LL), pelvic incidence (PI), pelvic tilt (PT), sagittal vertical axis (SVA), T1 pelvic angle (TPA) in sagittal plane, and cobb angle in coronal plane. Comparison was made between quasi-automatic and manual measurement.

Results: The mean age was 53.7±19.9 years old. In the whole population, the mean differences between the two methods were 3.9° for TK (30.5°±9.9° vs. 26.6°±9.3°, P<0.001), –5.2° for LL (–47.5°±11.2° vs. –42.4°±11.0°, P<0.001), 3.6° for PI (46.9°±10.3° vs. 43.9°±10.3°, P<0.001), –0.2° for PT (11.9°±7.7° vs. 12.0°±8.2°, P=0.328), –2.1 mm for SVA (15.7±26.2 vs. 17.8±26.3 mm, P=0.221) and –1.1° for TPA (9.0°±7.6° vs. 10.1°±7.8°, P=0.051). The deformity group had similar mean differences with the asymptomatic group with the values ranged from –4.1° to 3.8° for sagittal parameters. The mean differences of Cobb angle were 1.9° for patients with Cobb angle <30° and 2.3° for patients with Cobb angle >30°, respectively. Correlation analysis showed r² for all clinical parameters ranged from 0.667 to 0.923. On average, the new method takes 5 minutes to compute all the parameters for one case.

Conclusions: In conclusion, this ergonomic and efficient quasi-automatic method for full spine proved fast and accurate measurement in a large population, which showed great potential in extensive clinical application.
Introduction

Scoliosis is a complex three-dimensional (3D) deformity of the spine, which is characterized by a curvature in the coronal plane, which is usually quantified by Cobb angle, but also by a malalignment in the sagittal plane and rotation in the axial plane (1). 3D reconstruction techniques facilitate quantitative assessment, prognostication of deformity progression as well as assisting clinical management from bracing to surgical decision (2-4).

With the development of low-dose biplanar imaging system (EOS Imaging, Paris), 3D reconstruction of the thoracolumbar spine can be achieved with the bundled SterEOS software based on statistical modeling and bone shape recognition which is limited by the slow reconstruction and operator dependency. While endplate digitization is widely used for clinical parameters measurements (Cobb angle, kyphosis, lordosis), feedback from operators and radiology technicians is that manual adjustments of the 3D model is often required routinely. Previous studies reported that a number of radiographic parameters of the spine and pelvis, including thoracic kyphosis (TK), lumbar lordosis (LL), pelvic incidence (PI), pelvic tilt (PT), sagittal vertical axis (SVA) as well as T1 pelvic angle (TPA), play a role in pain and disability, and measuring health-related quality of life (HRQoL) in patients with spinal deformity (5-7). Therefore, there is a growing need to enhance the efficiency of the tedious daily measurement.

Recently, a quasi-automatic 3D reconstruction and measurement of spine has been proposed, which has been validated and proved fast and accurate in 57 patients with adolescent idiopathic scoliosis with less than 2.5 minutes per case, thus contributed a remarkable step towards full automatization of 3D reconstruction of the spine for wider applications (8). Nevertheless, 2D measurements are still considered the golden standard in clinical routine. Therefore, the objective of this study was to compare manual measured 2D spinopelvic parameters with those measured using the validated quasi-automatic 3D reconstruction measurements in a large cohort.

Methods

Subjects

A total of 494 adults aged from 20 to 89 years old who underwent biplanar X-ray scanning (EOS system, EOS Imaging, Paris, France) were included in this study, and divided into seven age groups (Table 1). Subjects were all interviewed by trained medical staffs following strict protocols with criteria. The exclusion criteria were as follows: (I) history of neuromuscular disorders or congenital anomalies; (II) previous spine, pelvis or lower-limb pathology that could affect the spine; (III) previous surgery on spine, pelvis or lower limb; or (IV) pregnancy (9). Then the subjects divided into asymptomatic (Group A) and scoliosis (Group S) group according to the presence of spinal deformity (Cobb angle >10°).

3D reconstruction

A quasi-automatic 3D reconstruction and measurement of the spine was carried out in four steps using previously proposed method (10). Briefly, the operator started by identifying the acetabula, sacral endplate and the spinal midline through the center of all vertebral bodies, from the tip of the odontoid process to L5, on the frontal and lateral radiographs. Secondly, the operator marked the upper endplate of C7 and lower endplate of T12 on the sagittal view, as well as the upper and lower end vertebrae of the scoliotic curve, when present, on coronal curve. Then, an automatic algorithm provided an initial solution of 3D reconstruction based on the method of transversal and longitudinal inferences (Figure 1) (11).

Radiographic parameters

The following radiographic parameters were automatically computed from the 3D reconstruction: TK, LL, PI, PT,
Table 1 Demographic distribution of study participants

<table>
<thead>
<tr>
<th>Parameters</th>
<th>Female (n=271)</th>
<th>Male (n=223)</th>
<th>Total (n=494)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age 20–29</td>
<td>41</td>
<td>31</td>
<td>72</td>
</tr>
<tr>
<td>Age 30–39</td>
<td>40</td>
<td>31</td>
<td>71</td>
</tr>
<tr>
<td>Age 40–49</td>
<td>39</td>
<td>32</td>
<td>71</td>
</tr>
<tr>
<td>Age 50–59</td>
<td>36</td>
<td>32</td>
<td>68</td>
</tr>
<tr>
<td>Age 60–69</td>
<td>38</td>
<td>33</td>
<td>71</td>
</tr>
<tr>
<td>Age 70–79</td>
<td>40</td>
<td>33</td>
<td>73</td>
</tr>
<tr>
<td>Age 80–89</td>
<td>37</td>
<td>31</td>
<td>68</td>
</tr>
<tr>
<td>Body height (cm)</td>
<td>158.9±6.2</td>
<td>168.3±6.5</td>
<td>163.8±6.4</td>
</tr>
<tr>
<td>Body weight (kg)</td>
<td>54.7±7.4</td>
<td>68.8±7.8</td>
<td>61.3±7.6</td>
</tr>
</tbody>
</table>

Figure 1 A bi-planar radiograph with posteroanterior and lateral view showed the 3D reconstruction procedures. 3D, three-dimensional.

SVA, TPA in sagittal plane, and cobb angle in coronal plane. The same parameters were also measured manually in 2D in the frontal and lateral radiographs. Comparison was made between quasi-automatic 3D and manual 2D measurement. The manual measurements were done by two orthopedic surgeons (LZ and TPL) with over 10 years of experiences. Intra- and inter-observer variations were conducted by two independent observers and estimated by using intra-class correlation coefficient (ICC), which were graded using previously described semi-quantitative criteria: excellent (ICC ≥ 0.9), good (0.7 ≤ ICC < 0.9), acceptable (0.6 < ICC ≤ 0.7), poor (0.5 ≤ ICC < 0.6), or unpredictable (ICC < 0.5).

Statistical analysis

All measurements were tabulated and analyzed using the SPSS version 22.0 software (SPSS Inc., Chicago, IL, USA). Normality of data distribution was checked with Kolmogorov-Smirnov test. Comparisons of mean values between quasi-automatic and manual measurements were performed using paired t-test if data was normally distributed or Mann-Whitney test (if data was not normally distributed). Bland-Altman analysis and Pearson correlations analysis were performed on the radiographic parameters between two measurements. Differences were detected as significant when a significance level (alpha) < 0.05 was calculated.
Table 2: Radiographic data of the two measurements

<table>
<thead>
<tr>
<th>Parameters</th>
<th>TK(^1)</th>
<th>TK(^2)</th>
<th>LL(^1)</th>
<th>LL(^2)</th>
<th>PI(^1)</th>
<th>PI(^2)</th>
<th>PT(^1)</th>
<th>PT(^2)</th>
<th>SVA(^1)</th>
<th>SVA(^2)</th>
<th>TPA(^1)</th>
<th>TPA(^2)</th>
<th>Cobb(^1)</th>
<th>Cobb(^2)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mean</td>
<td>30.5</td>
<td>26.5</td>
<td>-47.5</td>
<td>-42.4</td>
<td>46.9</td>
<td>43.3</td>
<td>11.9</td>
<td>12.0</td>
<td>15.7</td>
<td>17.8</td>
<td>9.0</td>
<td>10.1</td>
<td>33.5</td>
<td>31.4</td>
</tr>
<tr>
<td>SD</td>
<td>9.9</td>
<td>9.3</td>
<td>11.2</td>
<td>11.0</td>
<td>10.3</td>
<td>10.9</td>
<td>7.7</td>
<td>8.2</td>
<td>26.2</td>
<td>26.3</td>
<td>7.6</td>
<td>7.8</td>
<td>10.6</td>
<td>10.4</td>
</tr>
<tr>
<td>SE</td>
<td>0.5</td>
<td>0.4</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
<td>0.4</td>
<td>0.4</td>
<td>1.2</td>
<td>1.2</td>
<td>0.4</td>
<td>0.4</td>
<td>2.6</td>
<td>2.3</td>
</tr>
<tr>
<td>Min</td>
<td>-0.6</td>
<td>2.0</td>
<td>-79.2</td>
<td>-77.3</td>
<td>25.5</td>
<td>13.0</td>
<td>-10.8</td>
<td>-12.0</td>
<td>-70.8</td>
<td>-67.6</td>
<td>-10.3</td>
<td>-13.0</td>
<td>14.2</td>
<td>15.8</td>
</tr>
<tr>
<td>Max</td>
<td>71.2</td>
<td>63.0</td>
<td>17.5</td>
<td>21.0</td>
<td>89.2</td>
<td>91.0</td>
<td>40.4</td>
<td>43.0</td>
<td>134.2</td>
<td>130.6</td>
<td>40.0</td>
<td>53.5</td>
<td>51.3</td>
<td></td>
</tr>
</tbody>
</table>

\(^1\), measured by quasi-automatic method; \(^2\), measured by manual method. TK, thoracic kyphosis; LL, lumbar lordosis; SS, sacral slope; PT, pelvic tilt; PI, pelvic incidence; SVA, sagittal vertical axis; TPA, T1 pelvic angle.

Table 3: Comparison of the radiographic values between automatic measurement and manual measurement in the whole cohort

<table>
<thead>
<tr>
<th>Parameters</th>
<th>TK</th>
<th>LL</th>
<th>PI</th>
<th>PT</th>
<th>SVA</th>
<th>TPA</th>
<th>Cobb</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mean difference</td>
<td>3.9</td>
<td>-5.2</td>
<td>3.6</td>
<td>-0.2</td>
<td>-2.1</td>
<td>-1.1</td>
<td>2.1</td>
</tr>
<tr>
<td>Mean absolute error</td>
<td>5.3</td>
<td>6.8</td>
<td>5.0</td>
<td>1.6</td>
<td>4.5</td>
<td>2.1</td>
<td>2.7</td>
</tr>
<tr>
<td>SD absolute error</td>
<td>3.8</td>
<td>5.4</td>
<td>4.5</td>
<td>2.0</td>
<td>6.5</td>
<td>2.6</td>
<td>2.0</td>
</tr>
<tr>
<td>Coefficient of variation</td>
<td>19.0</td>
<td>15.2</td>
<td>11.2</td>
<td>13.2</td>
<td>25.4</td>
<td>21.0</td>
<td>18.7</td>
</tr>
<tr>
<td>Max absolute error</td>
<td>21.4</td>
<td>34.5</td>
<td>32.6</td>
<td>14.3</td>
<td>54.4</td>
<td>16.4</td>
<td>15.5</td>
</tr>
<tr>
<td>Percentage difference (%)</td>
<td>14.7</td>
<td>12.3</td>
<td>8.0</td>
<td>1.7</td>
<td>11.8</td>
<td>10.9</td>
<td>6.7</td>
</tr>
</tbody>
</table>

TK, thoracic kyphosis; LL, lumbar lordosis; SS, sacral slope; PT, pelvic tilt; PI, pelvic incidence; SVA, sagittal vertical axis; TPA, T1 pelvic angle.

Results

A total of 494 subjects (female/male: 271/223) were enrolled in this study with a mean age of 53.7±19.9 (range, 20–89) years old. Table 1 showed the age and gender distribution. The BMI was 24.1±6.8 kg/m\(^2\). Among this large population, 442 subjects were included in Group A, and 52 in Group S with a mean Cobb angle of 31.4°±10.4°. The intra- and inter-observer ICCs were from 0.667 to 0.923, which suggested a good to excellent reliability of these measurements between the two observers.

In the whole population, the comparison between the two measurements of the mean values of TK, LL, PI, PT, SVA and TPA was shown in Table 2. Mann-Whitney test showed the comparison between the two measurements as follows: TK (P<0.001), LL (P<0.001), PI (P<0.001), PT (P=0.328), SVA (P=0.221), TPA (P=0.051). The mean differences were 3.8° for TK, -5.1° for LL, 3.6° for PI, -0.1 for PT, -2.2 mm for SVA and -1.1° for TPA. The SD difference in LL was 7.7°, which was the largest among these parameters (Table 3).

In asymptomatic cohort, the mean differences between the two measurements were similar to the values in the whole population (Table 4). The mean differences of TK, LL, and PT in Group A was 0.1° higher than those in the whole population, while PI and TPA were the same between the two cohorts. The Group S had similar mean differences with the values ranged from -4.1° to 3.8° for sagittal parameters. In the coronal plane, the mean difference of Cobb angle between measurement methods was 1.9°, with a mean value of 1.6° for patients with Cobb angle <30° and 2.3° for patients with Cobb angle >30°, respectively.

Figure 2 shows Bland-Altman graphs for the agreement between the quasi-automatic and manual method for all sagittal parameters. Correlation analysis showed r\(^2\) for all radiographic parameters between two measurements ranged from 0.661 to 0.923 (Figure 3, P<0.01). For an experienced operator, it took 5 minutes in average to obtain the 3D reconstruction of spine and pelvis, while the time consumed in traditional manual measurement was 15 minutes.

Discussion

This study represented a large-scale cross-sectional
Table 4 Comparison of the radiographic values between automatic measurement and manual measurement in the asymptomatic group

<table>
<thead>
<tr>
<th>Parameters</th>
<th>TK</th>
<th>LL</th>
<th>PI</th>
<th>PT</th>
<th>SVA</th>
<th>TPA</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mean difference</td>
<td>3.8</td>
<td>-5.1</td>
<td>3.6</td>
<td>-0.1</td>
<td>-2.2</td>
<td>-1.1</td>
</tr>
<tr>
<td>Mean absolute error</td>
<td>5.4</td>
<td>6.8</td>
<td>5.1</td>
<td>1.6</td>
<td>4.6</td>
<td>2.1</td>
</tr>
<tr>
<td>SD absolute error</td>
<td>3.7</td>
<td>5.2</td>
<td>4.3</td>
<td>2.1</td>
<td>6.5</td>
<td>2.5</td>
</tr>
<tr>
<td>Coefficient of variation</td>
<td>18.8</td>
<td>15.2</td>
<td>11.1</td>
<td>13.2</td>
<td>25.4</td>
<td>21.0</td>
</tr>
<tr>
<td>Max absolute error</td>
<td>22.5</td>
<td>34.1</td>
<td>33.3</td>
<td>14.8</td>
<td>54.0</td>
<td>15.9</td>
</tr>
</tbody>
</table>

TK, thoracic kyphosis; LL, lumbar lordosis; SS, sacral slope; PT, pelvic tilt; PI, pelvic incidence; SVA, sagittal vertical axis; TPA, T1 pelvic angle.

Figure 2 Bland-Altman plots for the agreement between the quasi-automatic and manual measurements for TK, LL, PI, PT, SVA and TPA. TK, thoracic kyphosis; LL, lumbar lordosis; PI, pelvic incidence; PT, pelvic tilt; SVA, sagittal vertical axis; TPA, T1 pelvic angle.

A comparative analysis of quasi-automatic 3D measurement of full spine derived from EOS biplanar standing radiographs aged from 20 to 89 years old. Based on the findings, this new technique of quasi-automatic 3D reconstruction and measurement proved fast in a large population with a wide variety of spine morphologies across different ages. Furthermore, the geometrical parameters calculated from 3D reconstruction were consistent with 2D manual measurements.

The scientific and clinical importance of 3D reconstruction and measurement of the spine is largely increasing in recent years with the development of EOS biplanar low-dose X-ray radiography (11,12). To have a better understanding of the initiation and progression of scoliosis as well as the optimistic surgical decision-making, the new 3D classification of AIS and key 3D index were proposed in recent years (2,13-15). However, the complexity and operator dependency of the original reconstruction method limited its extensive application in clinical routine. The novel approach allows for an accurate 3D reconstruction with a much shorter operator-time.

The Cobb angle measurement is calculated from the coronal spinal curvature, which is important to determine the curve pattern, severity of scoliosis and treatment...
strategy. Therefore, an accurate measurement of Cobb angle is indispensable. In the current study, consistency between 2D and 3D Cobb angle measurements was tested; differences in Group S were 1.9° in patients with Cobb angle smaller than 30° and 2.3° in patients with Cobb angle larger than 30°. Sardjono et al. reported an automatic Cobb angle determination and tested the accuracy in 36 AIS patients with a mean difference of 3.3° (16). In a recent study, Zhang et al. proposed an automatic method for Cobb angle measurement and compare the results with 2D manual measurement in which the mean differences were 2.9° in mild group (Cobb angle <25°), 3.7° in moderate group (Cobb angle between 25° and 45°) and 3.9° in severe group (Cobb angle <45°), respectively (17). In addition, Safari et al. newly developed a semi-automatic algorithm to estimate Cobb angle, which was user-friendly and reliable with a correlation coefficient of 0.81 (18).

On the other hand, a number of studies have shown that the sagittal parameters of the spine and pelvis play an important role in evaluating HRQoL in patients with spinal deformity (5-7). Safari et al. developed a deep learning tool for automatic measurement of sagittal parameters, and the results showed that the mean differences with manual measurements were for 5.5° PI, 2.7° for PT and 5.0° for spinosacral angle (18). Nevertheless, TK and LL were not assessed in their study; these parameters are difficult to estimate through automatic identification due to the low visibility at upper thoracic vertebrae overlapped by upper arm and lower lumbar vertebrae obstructed by iliac crest and intestine contents in the sagittal view. Galbusera et al. recently conducted a study of automatic analysis of spinal deformities, which presented that the standard deviation of TK and LL were 8.6° and 11.5°, respectively (19). By contrast, the current study showed that the SD of TK and LL were 5.3° and 6.8°, respectively, which revealed a good measurement performance in sagittal parameters, although disagreement between 2D and 3D LL was relatively high. This might be due to the shape and visibility of the sacral plateau, which can be difficult to digitize with a straight line, as it is done in the 2D measurement.

In addition to other angular sagittal parameter, the linear parameter SVA, which correlates with pain and poor HRQoL scores (20) was also validated in this study with a mean difference of –2.1 mm. Another study of automatic measurement for SVA reported the mean absolute error between automatic and manual methods ranged from 1.18 to 9.82 mm (21). As a global angular parameter, TPA quantifies spinopelvic malalignment and compensation through pelvic retroversion, which is not influenced by various postural compensatory mechanisms (22,23). To the best our knowledge, this is the first study to develop a quasi-automatic measurement for TPA, and the mean difference was only –1.1°.

This new method of quasi-automatic reconstruction and measurement, which was based on statistical inferences, image processing and machine learning, greatly reduce the time-consuming work of manual measurement on radiographs or adjusting each vertebra manually via elastic

Figure 3 Scatter plots for correlation analysis in all radiographic parameters.
deformation for orthopedic surgeon and scientists (10). It took less than 5 minutes on average to generate a 3D reconstruction of pelvis and spine; this reconstruction allows the automatic computation of parameters on coronal, sagittal and axial plane. However, once the reconstruction is available, computation for novel parameters, such as TPA, can easily be implemented. On the other hand, manual 2D measurement usually takes more than 15 minutes to complete all the parameters ever for a well-trained operator (24), and the acquired measurements cannot be exploited further. In this study, the cohort was comprised of a variety of spine morphologies across wide age distribution, which proved the accuracy and clinical applicability of the proposed method in a large of young and elder, scoliotic and asymptomatic subjects.

However, there were still some limitations in this study. The proposed method as well as other automatic methods have natural difficulty in recognizing malformed vertebrae, thus the capacity of reconstruction and measurement for congenital and severe degenerative spinal deformity needs further improvement. Such cases were not included in this study. While a fully automatic method is ultimate goal in the upcoming era of artificial intelligence, the proposed method combining automatic processing and soft manual adjustment could be considered as a cogitative trade-off between automation and accuracy.

In conclusion, this ergonomic and efficient quasi-automatic method for full spine proved fast and accurate measurement in a large population, which showed great potential in extensive clinical application.

**Acknowledgments**

The authors are grateful to the ParisTech BiomecAM chair program on subject-specific musculoskeletal modelling (with the support of ParisTech and Yves Cotrel Foundations, Société Générale, Proteor and Covea).

**Funding:** None.

**Footnote**

*Conflicts of Interest:* All authors have completed the ICMJE uniform disclosure form (available at http://dx.doi.org/10.21037/qims-20-861). The authors have no conflicts of interest to declare.

*Ethical Statement:* This study was approved by the Joint Chinese University of Hong Kong-New Territories East Cluster Clinical Research Ethics Committee (CREC Ref. No. 2017.689) and all participants provided written informed consent.

**Open Access Statement:** This is an Open Access article distributed in accordance with the Creative Commons Attribution-NonCommercial-NoDerivs 4.0 International License (CC BY-NC-ND 4.0), which permits the non-commercial replication and distribution of the article with the strict proviso that no changes or edits are made and the original work is properly cited (including links to both the formal publication through the relevant DOI and the license). See: https://creativecommons.org/licenses/by-nc-nd/4.0/.

**References**