Usefulness of enhancement-perfusion mismatch in differentiation of CNS lymphomas from other enhancing malignant tumors of the brain

Pradeep Goyal1, Yogesh Kumar2, Nishant Gupta3, Ajay Malhotra4, Saurabh Gupta5, Sonali Gupta6, Manisha Mangla1, Rajiv Mangla2

1Department of Radiology, St. Vincent's Medical Center, Bridgeport, Connecticut, USA; 2Department of Radiology, Columbia University at Bassett Healthcare, Cooperstown, New York, USA; 3Department of Radiology, Columbia University Medical Center, New York, NY, USA; 4Department of Radiology and Biomedical Imaging, Yale School of Medicine, New Haven, Connecticut, USA; 5Department of Radiology, SUNY Upstate Medical University, Syracuse, New York, USA; 6Department of Medicine, St. Vincent's Medical Center, Bridgeport, Connecticut, USA; 7Department of Radiology, University of Rochester Medical Center, Rochester, New York, USA

Correspondence to: Pradeep Goyal, MD. Department of Radiology, St. Vincent's Medical Center, Bridgeport, CT 06606, USA.
Email: pradeepgoyal78@gmail.com.

Background: Surgical planning and treatment options for primary or secondary central nervous system lymphomas (PCNSL or SCNSL) are different from other enhancing malignant lesions such as glioblastoma multiforme (GBM), anaplastic gliomas and metastases; so, it is critical to distinguish them preoperatively. We hypothesized that enhancement-perfusion (E-P) mismatch on dynamic susceptibility weighted magnetic resonance (DSC-MR) perfusion imaging which corresponds to low mean relative cerebral blood volume (mean rCBV) in an enhancing portion of the tumor should allow differentiation of CNS lymphomas from other enhancing malignant lesions.

Methods: We retrospectively reviewed pre-treatment MRI exams, including DSC-MR perfusion images of 15 lymphoma patients. As a control group, pre-treatment DSC-MR perfusion images of biopsy proven 18 GBMs (group II), 13 metastases (group III), and 10 anaplastic enhancing gliomas (group IV) patients were also reviewed. Region of interests (ROIs) were placed around the most enhancing part of tumor on contrast-enhanced T1WI axial images and images were transferred onto co-registered DSC perfusion maps to obtain CBV in all 4 groups. The mean and maximum relative CBV values were obtained. Statistical analysis was performed on SPSS software and significance of the results between the groups was done with Mann-Whitney test, whereas optimal thresholds for tumor differentiation were done by receiver operating characteristic (ROC) analysis.

Results: The enhancing component of CNS lymphomas were found to have significantly lower mean rCBV compared to enhancing component of GBM (1.2 versus 4.3; P<0.001), metastasis (1.2 versus 2.7; P<0.001), and anaplastic enhancing gliomas (1.2 versus 2.4; P<0.001). Maximum rCBV of enhancing component of lymphoma were significantly lower than GBM (3.1 versus 6.5; P<0.001) and metastasis (3.1 versus 4.9; P<0.013), and not significantly lower than anaplastic enhancing gliomas (3.9 versus 4.2; P<0.08). On the basis of ROC analysis, mean rCBV provided the best threshold [area under the curve (AUC) =0.92] and had better accuracy in differentiating malignant lesions.

Conclusions: E-P mismatch in DSC perfusion MR, i.e., low mean rCBV in an enhancing portion of the tumor is strongly suggestive of lymphoma and should allow differentiation of CNS lymphoma from other enhancing malignant lesions.

Keywords: CNS lymphoma; glioblastoma multiforme (GBM); dynamic susceptibility weighted magnetic resonance perfusion imaging (DSC-MR perfusion imaging); enhancement-perfusion mismatch (E-P mismatch)

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Introduction

CNS lymphoma, glioblastoma multiforme (GBM), grade III enhancing tumors and metastasis are the common enhancing malignant brain tumors. Differentiating the above mentioned malignant tumors can be a challenge on routine MR imaging because of overlapping imaging findings (1). It is critical to distinguish CNS lymphomas from other enhancing malignant lesions preoperatively due to distinct prognostic implications and differing surgical planning and treatment options. Moreover, appropriate preoperative diagnosis of CNS lymphoma helps in averting needless surgical removal due to lack of survival benefits and increase in postoperative morbidities (2).

Indexed literature has proved promising role of utilizing advanced imaging techniques to help differentiation between the previously mentioned tumors. Dynamic susceptibility weighted magnetic resonance (DSC-MR) perfusion imaging is a fast and powerful functional MR technique, whose application is gaining ground in assessing intracranial tumors likely due to increasing availability of better hardware and software (3). Data provided by DSC perfusion MR imaging include physiological aspects of angiogenesis, vascular density and vascular endothelial proliferation (4,5). DSC-MR perfusion imaging is useful in characterization of tumor aggressiveness by evaluating tumor microcirculation and hemodynamics based on tumor neovascularization and endothelial hyperplasia (6). Relative cerebral blood volume (rCBV) is a most commonly used parameter in DSC-MR perfusion imaging. Several studies have shown, increase in the micro-vasularity and neo-vasularity of malignant intracranial masses correlate with high rCBV. GBM and high-grade gliomas have high rCBV due to rigorous neo-vascularity (6-8). Lymphomas were found to be associated with lower rCBV values (5,9,10). The rCBV values of lymphoma are noted to be much less compared to high-grade gliomas (11,12). Few earlier studies highlighted salient features of enhancing malignant lesions based on rCBV measurements on DSC perfusion and with diffusion (DWI-ADC), but were not always confirmatory (9,13). In previous studies, rCBV was chosen in the regions of interest with the maximum microvascular and neo-vascular density, which should represent the max rCBV. Several other techniques such as time-dependent leakage [permeability transfer constant (Ktrans)] reflecting leakiness on a T1W dynamic contrast-enhanced (DCE) perfusion, and fractional blood plasma volume per unit volume of tissue (Vp) reflecting perfusion have been used to measure perfusion-related parameters. DCE perfusion was also found effective in differentiating primary central nervous system lymphomas (PCNSL) from GBM (14,15). More recent studies have suggested the moderate effectiveness of DCE perfusion imaging for differentiation of GBM and PCNL (16).

However, the purpose of current study is to further explore the imaging role of DSC-MR perfusion. We hypothesized that enhancement-perfusion (E-P) mismatch on DSC perfusion imaging as measured by low mean rCBV in an enhancing portion of the tumor should allow differentiation of lymphomas from other enhancing malignant lesions.

Methods

Patient selection

This retrospective study group included 15 patients (13 biopsy proven primary and 2 secondary) and CNS lymphomas (10 males and 5 females), from July 2011 to December 2014. Inclusion criteria included the patients with parenchymal CNS lymphoma for which optimum pretreated DSC perfusion imaging were available. As a control group, histopathology proven matched 18 GBM (group II), 13 solitary intracranial metastases (group III), and 10 anaplastic enhancing gliomas (group IV) patients with optimum pretreatment DSC perfusion images were included from the same time period. Metastases were from lung (n=8), esophagus (n=2), breast (n=2) and melanoma (n=1) primaries. Inclusion criteria included only the patients with enhancing lesions on imaging and without prior treatment.

Imaging protocol

Various MR imaging sequences were obtained on a 1.5/3 T MR scanner (Signa LX Scanner, and Discovery™ 750; GE Healthcare, Milwaukee, Wisconsin, USA) with the help of standard 8-channel head coil. Conventional sequences included axial T1 FSE, T2FLAIR, T2 FSE, and gradient recalled echo (GRE). Post-contrast T1-weighted images in 3 planes were obtained following acquisition of DSC imaging. DSC images were acquired with T2* (gradient-echo planar) sequence using parameters which include: matrix size =128x96, section thickness =6 mm without gap, NEX 1, TR/TE =1,500/50 ms and flip angle =80°. Before starting the contrast agent injection, initial first 10
acquisitions in a total of 60 image volumes were selected to establish a pre-contrast baseline. After acquisition of the first 10 image volumes, a total of 0.15 mmol/kg of body weight gadopentetate dimeglumine was injected at a rate of 5 mL/s followed by a 20 mL bolus of saline injection at the same rate of 5 mL/s through an 18- or 20-G intravenous catheter. A total of 12 contiguous axial sections were chosen for the analysis on the basis of lesion extent determined by the pre-contrast T2 FLAIR images.

**Post processing and perfusion measurements**

**rCBV measurement**

Post-processing of images was conducted on a different workstation by author (R Mangla), who was blinded from the histologic findings at the time of analysis. Reference was made with conventional imaging during calculation of rCBV. Region of interests (ROIs) were drawn around the most enhancing part of tumor on contrast-enhanced T1WI axial images and images were transferred onto co-registered DSC perfusion maps multiple ROIs of 20–50 mm$^2$ were drawn over 4 or 5 hot perfused spots, and the highest value i.e., max rCBV was picked (Figure 1A). This method has been shown to have a better inter- and intra-observer agreement (4). Raw data of perfusion images as well as T1- and T2-weighted images were used to ensure that regions of interest did not include apparent blood vessels or any hemorrhage. For normalization, another ROI with approximate size of 20–50 mm$^2$ was drawn in the contralateral normal-appearing white matter as a standard internal reference. In this way, CBV measurements become a relative measure and are called rCBV. After that, rCBV ratio was obtained by dividing the rCBV values of lesion from the contralateral normal-appearing white matter. Similarly, mean rCBV was measured in the section with the largest enhancing dimensions and a ROI was placed to cover almost the entire portion of the tumor (Figure 1B). More the E-P mismatch, lower the mean rCBV.

**Statistical analysis**

Various perfusion parameters were analyzed for diagnostic accuracy by using SAS, Version 9.4 (SAS Institute, Cary, North Carolina, USA) and the IBM SPSS statistics, Version 22.0 (IBM, Chicago, Illinois, USA) software. Significance of the results between the groups was tested by Mann-Whitney test. Receiver operating characteristic (ROC) was analyzed for various perfusion parameters with statistically significant differences in regard to their ability to differentiate lymphoma from GBM, lymphoma from metastases and lymphoma from anaplastic enhancing tumors. The area under the curve (AUC) was computed to determine most predictive continuous variables among max rCBV and mean rCBV for diagnosing lymphomas.

**Results**

The mean rCBV and max rCBV of lymphomas, GBMs, metastases and anaplastic enhancing malignant tumors are summarized in Figures 2, 3 respectively. Representative
PCNSL and GBM cases are shown in Figures 4, 5. The enhancing components of CNS lymphomas were found to have significantly lower mean rCBV (E-P mismatch) compared to enhancing component of GBM (1.2 versus 4.3; P<0.001) (Table 1; Figure 2), metastasis (1.2 versus 2.7; P<0.001) (Table 1; Figure 3), and anaplastic enhancing tumors (1.2 versus 2.4; P<0.001) (Table 1; Figure 2). Maximum rCBV of enhancing component of lymphomas were also low but only significantly lower than GBM (3.1 versus 6.5; P<0.001) (Table 1, Figure 3) and metastasis (3.1 versus 4.9; P<0.013) (Table 1; Figure 3) but not with anaplastic enhancing tumors (3.9 versus 4.2; P<0.08) (Table 1; Figure 3). On the basis of ROC analysis, mean rCBV provided the best threshold (AUC =0.92) and had better accuracy in differentiating malignant lesions (Figure 6). Table 2 shows the sensitivity and specificity of mean rCBV (E-P) in differentiating these lesions. In our study, low mean rCBV (E-P mismatch) had better sensitivity (90%) and specificity (91%) with a cut-off <1.7 in differentiating lymphoma from other malignant intracranial lesions.

**Discussion**

Diagnosis of lymphoma pre-operatively is crucial due to distinct prognostic implications and differing surgical planning and treatment options, as well as to guide for biopsy (17,18). Steroid administration prior to histological diagnosis of brain tumors, can result in decreased diagnostic yield for resection or stereotactic biopsies, therefore making it imperative to recognize lymphoma by imaging (19). Despite similar MR imaging findings, significant structural differences in the tumor capillaries have been documented
on reported histological studies (20). Differences in angio-architecture cause variability in DSC-MR perfusion parameters such as rCBV, which reflects the micro-vessel density (MVD), and PSR (perfusion signal intensity recovery which is measured at the end of contrast agent first pass, compared to baseline) as well as in DCE-MRI parameter such as $K^{trans}$, which is the coefficient of volume transfer denoting vascular permeability and can help in differentiating these tumors.

DSC-MR perfusion imaging is based on a first-pass bolus imaging technique, which relies on the susceptibility induced signal loss on T2* weighted sequences resulting from a bolus of gadolinium-based contrast passing through a capillary bed. This is generally used to estimate rCBV in brain tumor studies, which can reflect tumor vascular morphometry (21). On DSC-MR perfusion imaging, gadolinium leaks into the interstitial spaces of the enhancing tumors and therefore, alters the microenvironment and subsequently signal-intensity recovery curve shape. T1 effects result in higher signal-intensity recovery, while T2* effects result in lower signal-intensity recovery (22). Due to complex interplay of multiple mechanisms at the time of passage of gadolinium as well as after passage of gadolinium during PSR and $K^{trans}$ measurements (23), there was a need of simpler parameter for assessing permeability.

It has been documented that area with maximal-rCBV does not correspond to the area of highest permeability and only modest correlation has been found between max rCBV and $K^{trans}$ (4). Microvascular area (MVA), that encompasses both the number and the caliber of the micro vessels, can provide a better estimation of the whole vascular surface area and represents a better and definite measure of the degree of angiogenesis (24). Perfusion has been shown to have high correlation with the MVA and poor correlation with permeability (25). However, permeability has shown moderate correlation with maximal enhancement (25). Based on the above facts, it was presumed that another simple parameter of DCS perfusion imaging should be evaluated which accounts for both perfusion and permeability. We hypothesized that E-P mismatch in an enhancing portion of the tumor, which is represented by low mean rCBV on DCS perfusion imaging, should allow differentiation of enhancing malignant lesions. Indeed in our study, we found that CNS lymphomas can be differentiated from other enhancing malignant lesions based on E-P mismatch.

### Differentiating lymphoma from GBM and anaplastic enhancing tumors

In our study, lymphomas were found to have lower max rCBV values than high-grade gliomas, similar to previous studies (9-12). However, max rCBV values of anaplastic enhancing tumors were not significantly different from max rCBV of lymphomas (4.16 vs. 3.09, $P<0.08$). Lymphomas have unique angiocentric growth patterns with invasion of lumen vessel as well as endothelial cells with paucity of neoangiogenesis and small extravascular extracellular space (26), resulting in less MVA and hence low perfusion. Also, frank endothelial discontinuities (due to thin and fenestrated endothelial cells) lead to high permeability resulting in frequently noted intense gadolinium enhancement in CNS lymphomas (27). Thus, lymphomas should have high E-P mismatch, as evident by statistically significant lower mean rCBV compared to GBMs and anaplastic tumors in our studies. GBMs have fragile neo-capillaries, disrupted blood brain barrier and vascular hyperplasia however, the MVA has been found to be less than anaplastic glioma due to lack of endothelial proliferation (22,23,28). These peculiar angio-architectures result in high perfusion and relatively low enhancement in anaplastic tumors compared to GBMs, as evident by more E-P mismatch or relatively lower mean rCBV values in anaplastic tumors compared to GBMs but significantly higher mean rCBV values compared to lymphomas in our study. In summary, lymphomas were difficult to differentiate from anaplastic gliomas on the basis of max rCBV; however, mean rCBV was useful.

### Differentiating lymphoma from metastasis

Metastatic lesions show fenestrations in their tumor capillaries corresponding to primary systemic cancers with lack of blood-brain barrier, leading to high permeability (29). It has been found that max rCBV of an enhancing mass stands as a good criterion to differentiate metastases from lymphoma and GBM (30). In our study, there was significant difference in both max rCBV (3.09 vs. 4.95, $P<0.013$) and mean rCBV (1.22 vs. 2.7; $P<0.001$) values of lymphomas and metastases. However, mean rCBV proved to be more robust than max rCBV in differentiation.

### Limitations

This retrospective study has several limitations. Many of our patients were treated with steroids based on clinical
Figure 4 Primary CNS lymphoma (PCNL): (A-D) enhancing lesion in left temporal lobe with significant edema without showing restricted diffusion may be suggestive of high grade tumor; (E) the max rCBV shows an area of increased perfusion (blue arrow) which makes it difficult to differentiate from other malignant lesions; (F) showing E-P mismatch; (G) H&E stain showing vessel and lymphoma cells; (H) highlights the vessels seen in the H&E with CD34 vascular marker. Paucity of neo-angiogenesis (G and H) helped in differentiation of lymphoma from other malignant tumors. rCBV, relative cerebral blood volume; E-P, enhancement-perfusion.
indications, which may affect the perfusion parameters. Technical limitations such as susceptibility artifacts related to hemorrhage, can lead to miscalculations in rCBV. Also, MR acquisition protocol can affect rCBV. A few lesions were assumed to be metastases based on primary neoplasm at other sites, without histopathology correlation. We want to mention that the reported results are purely observational using the proposed protocol using image processing methods in a small number of patients with lymphomas, GBMs, metastases, anaplastic gliomas.

**Conclusions**

DSC-perfusion MR imaging can be useful in differentiation
of lymphoma from other enhancing malignant brain tumors. Pretreatment mean and max rCBV were found to be low in lymphomas when compared to other enhancing malignant brain tumors in the present study. ROC showed that mean rCBV (E-P mismatch) had better sensitivity (90%) and specificity (91%) with a cut-off <1.7 in differentiating lymphoma from other malignant brain tumors.

Acknowledgements

None.

Footnote

Conflicts of Interest: The authors have no conflicts of interest to declare.

Ethical Statement: The study was approved by University of Rochester Medical Center Ethical Committee (No. RSRB00023950) and written informed consent was obtained from all patients.

References


Table 2 Sensitivity and specificity of mean rCBV (E-P) and max rCBV

<table>
<thead>
<tr>
<th>Type of rCBV</th>
<th>Threshold</th>
<th>Sensitivity</th>
<th>Specificity</th>
</tr>
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<tbody>
<tr>
<td>Mean rCBV (E-P)</td>
<td>&lt;1.69</td>
<td>90%</td>
<td>91%</td>
</tr>
<tr>
<td>Max rCBV</td>
<td>&lt;3.09</td>
<td>85%</td>
<td>67%</td>
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rCBV, relative cerebral blood volume.


